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(54) Title: SIMULTANEOUS PARTICLE SEPARATION AND CHEMICAL REACTION		
(57) Abstract <p>This invention provides a method and apparatus for detecting the presence of analyte particles in a sample fluid also comprising larger particles, particularly blood. It exploits diffusion to provide simultaneous filtering of the larger particles and reaction of the analyte particles. A sample stream and a reagent stream join on the upstream end of a laminar flow reaction channel and flow in adjacent laminar streams. The reagents can be in solution or immobilized on a bead. The analyte particles diffuse from the sample stream into the reagent stream, leaving behind the larger particles in the residual sample stream. In the reagent stream the analyte particles react with reagent particles and form product particles, thereby creating a product stream. At the downstream end of the reaction channel, the residual sample stream and the product stream are divided. The product particles are then detected, preferably optically, in the product stream. Prior to detection, the product stream can undergo further filtering or separation, or can join a second reagent stream to form secondary product particles. This apparatus and method can be used to implement competitive immunoassays or sandwich immunoassays using enzymatically or fluorescently labeled immunoreagents. The apparatus and method can also be used to synthesize products, in which case two reagent streams join in the laminar flow reaction channel.</p>		

SIMULTANEOUS PARTICLE SEPARATION AND CHEMICAL REACTION

FIELD OF THE INVENTION

This invention relates to simultaneous diffusion based filtering and chemical reaction of analytes in streams containing both these analytes and larger particles. The invention is useful, for example, for analyzing blood to detect the presence of small particles such as antigens in a stream containing cells, or for preparing small volumes of fluid products.

BACKGROUND OF THE INVENTION

It is possible to fabricate intricate fluid systems with channel sizes as small as a micron. These devices can be mass-produced inexpensively and are expected to soon be in widespread use for simple analytical tests. However, in chemical analysis of turbid fluids, notably blood, filtering of the larger particles such as cells is generally required prior to analysis, especially optical analysis. In clinical laboratories this is generally accomplished by centrifugation. The centrifugal force generated is a function of distance from the center, and thus centrifugation is not effective in a small scale apparatus. In chemical laboratories membrane filters are used to separate the larger particles. This can be used in microscale apparatus, but clogging of the filters with use makes them impractical.

The greater diffusion of small particles relative to larger particles can be used to partially separate the species. Diffusion is a process which can easily be neglected at large scales, but rapidly becomes important at the microscale. Due to extremely small inertial forces in such structures, practically all flow in microstructures is laminar. This allows the movement of different layers of fluid and particles next to each other in a channel without any mixing other than diffusion. Moreover, due to the small lateral distances in such channels, diffusion is a powerful tool to separate molecules and small particles according to their diffusion coefficients, which is usually a function of their size.

The present invention exploits diffusion to provide simultaneous filtering and chemical reaction, which facilitates the elimination of preprocessing of specimens containing particulate constituents, thus reducing the sample size and analytical time required.

SUMMARY OF THE INVENTION

This invention provides a method and apparatus for reacting small particles in a fluid also comprising larger particles. It provides simultaneous filtering of the larger particles and reaction of the small particles. The reactor can be followed by collection of or detection of the reaction products. The reactor exploits diffusion to separate the small primary particles from the larger particles. It utilizes microscale channels wherein diffusion becomes a significant factor and wherein the fluid flow is laminar. The reactor can be simply and inexpensively manufactured and can be disposed of after use. The reactor is capable of processing a fluid volume between about 0.01 microliters and about 20 microliters within a few seconds. Operation with sub-microliter volumes of sample fluid is a particular advantage for expensive reagents or for blood analysis. Larger volumes with correspondingly longer times can be used when preferred, for example viral detection in a sample with a low viral load.

The reactor can be used for analysis, in which case the inlet fluid, termed generically the primary fluid, is a sample fluid and the small particles, termed generically the small primary particles, are analyte particles. In this case the reactor is generally coupled with a detector. Alternatively, the reactor can be used to rapidly synthesize small volumes of product fluids. In this case the primary fluid is a reagent fluid and the small primary particles are reagent particles. This has particular application to making products starting from natural substances. In the following, the reactor is described for the analysis embodiment, but the description also applies to the synthesis embodiment.

The invention uses an "H" shaped reactor. In the H-reactor the crossbar of the H is a laminar flow reaction channel. On the upstream end of the crossbar a sample (primary) stream and a reagent stream enter through separate arms of the H, and the sample stream and the reagent stream flow in adjacent laminar streams in the crossbar. Because the flow is laminar, there is no turbulent mixing of the two streams, but the analyte particles diffuse from the sample stream into the reagent stream, leaving behind the larger particles in the residual sample stream. In the reagent stream the analyte particles react with reagent particles and form product particles, thereby creating a product stream. At the downstream end of the crossbar, the residual sample stream and the product stream divide into the two downstream arms of the H. The product particles can then be detected in the product stream.

Detection of the product particles can be performed using optical, electrical, chemical, electrochemical or calorimetric analysis, or any other technique in the analytical art. More than one detection technique can be used in the same system. The preferred embodiments use optical analysis or a combination of electrochemical and optical analysis. In optical detection, the product stream can be analyzed by luminescence, fluorescence or absorbance. To increase the signal in the detection zone the product stream channel can be broadened or convoluted. The product stream can connect to a flow cytometer for analysis, particularly a flow cytometer having a microfabricated flow channel.

An example of an application of this method is in competitive immunoassays in solution. The sample stream is whole blood containing native antigens. The reagent particles are antibodies bound to a fluorescently labeled antigen. In the reaction channel, the native antibodies diffuse into the reagent stream and displace the fluorescently labeled antigens. The product stream contains both native and fluorescently labeled antigens, some of which are free and some of which remain bound to antibodies. The relative amounts of free and bound fluorescently labeled antigen, which is a function of the amount of native antigen in the blood, can be measured.

Prior to detection, the product stream can undergo further filtering or separation. In particular the product stream can join with an extraction stream in a separation channel, such that the product and extraction streams flow in adjacent laminar flow streams. Smaller particles in the product stream flow into the extraction stream for detection, preferably optical detection.

An example of utilizing the separating channel is a competitive immunoassay as above wherein the antibody-fluorescently labeled antigen complex is immobilized on a microbead. In the separation channel, the free and bound fluorescently labeled antigen can be separated by diffusion. The free antigen that enters the extraction stream can be detected by fluorescence without interference from the antigen on the beads. In lieu of differential separation, the product stream can be coupled with a flow cytometer to measure the fluorescence intensity remaining on the beads. The bead can be magnetic, and a magnetic field can be used to pin the bead in the sample stream to allow reaction with the analyte particles. Following reaction, a reverse field returns the beads to the reagent stream.

The detection process can use a second reagent stream that joins with the product stream in a "T" configuration. The two streams flow in adjacent laminar streams, and small product particles from the product stream diffuse into the second reagent stream, or small reagent particles from the second reagent stream diffuse into the product stream. Depending on the diffusion process, in either or both streams the product particles react with the second reagent particles to form secondary product particles. The secondary product particles are detected as described above for primary product particles.

First and second reagent streams are useful, for example, for sandwich immunoassays. The first reagent is a primary antibody which binds to an antigen from the sample to form a first product. The first reagent is large enough to change the diffusion coefficient of the complex. The second reagent is a fluorescently labeled secondary antibody which reacts with the first product to form a sandwich complex. The complex is detected as described above for primary products. The slower diffusion of the complexed relative to the uncomplexed labeled antibody is used to distinguish between the two, either by diffusional separation of the species or by the extent of depolarization of the fluorescence.

Second reagent streams are also utilized when the first reaction involves an enzymatically labeled rather than fluorescently labeled reagent. The difference in enzymatic activity of bound and unbound enzymatically labeled reagent particles allows measurement of the extent of reaction. Through the second reagent stream, a substrate which is sensitive to the enzyme joins the first reaction products. Reaction of the substrate and enzyme is then detected as described above for primary products.

The first or subsequent product streams can flow through a delay line to allow the reaction to be completed before detection or before joining a subsequent reagent stream. The first or subsequent product streams can also undergo filtering or diffusional separation before detection or before joining a subsequent reagent stream. The reagents can be immobilized on magnetic beads, and a magnetic field can be used to pin the beads for reaction or flushing steps in any of the reaction channels.

The sample stream may be any stream containing an analyte and also containing less diffusive particles, for example blood or other body fluids, contaminated drinking water, contaminated organic solvents, biotechnological process samples, e.g., fermentation broths, and the like. The analyte can be any smaller particle in the sample stream which is capable of diffusing into the reagent stream faster than the larger particles, so as to substantially leave the larger particles in the residual sample stream. Examples of analyte particles are hydrogen, calcium, sodium and other ions, dissolved oxygen, proteins such as albumin, organic molecules such as alcohols and sugars, drugs such as salicylic acid, halothane and narcotics, pesticides, heavy metals, organic and inorganic polymers, viruses, small cells and other particles. In the preferred embodiment wherein the sample stream is whole blood, small particles such as antigens diffuse rapidly across the channel, whereas larger particles such as blood cells diffuse slowly.

The larger particles in the sample stream may also be sensitive to the reagent. Because these do not diffuse into the reagent stream, they do not interfere with detection of the analyte. By diffusion of the analyte but not the larger particles, cross-sensitivities of reagents to larger sample components, a common problem, can be avoided. Furthermore, the reagent can be kept in a solution in which it displays its optimal characteristics. For example, cross-sensitivities to pH or ionic strength can be suppressed by using strongly buffered reagent solutions.

BRIEF DESCRIPTION OF THE DRAWING

FIG. 1, comprising FIGS. 1a-b, is an H reactor illustrated with a competitive immunoassay. The reactor is shown in (a) plan view and (b) cross section.

FIG. 2 is an H reactor illustrated with a sandwich immunoassay.

FIG. 3 is an H reactor illustrated with a competitive immunoassay wherein the antibody is immobilized on a bead.

FIG. 4 is an H reactor illustrated with a competitive immunoassay wherein the antibody is immobilized on a magnetic bead and wherein a magnetic field is applied to pin the beads to one side of the reaction channel.

FIG. 5 is a convoluted detection channel for optical detection.

FIG. 6 is a broadened detection channel for optical detection.

FIG. 7 is a T separator for use with optical detection.

FIG. 8 is a single particle detection channel for use with optical detection.

5 FIG. 9 is an H reactor with a first reagent inlet followed by a T reactor with a second reagent inlet, illustrated with a sandwich immunoassay.

FIG. 10 is a T reactor for use in combination with an H reactor, illustrated with the reaction of an enzymatically labeled antigen.

10 FIG. 11 is an H filter and a T reactor for use in combination with an H reactor, illustrated with a sandwich immunoassay with subsequent selection of the sandwich complex, followed by reaction of an enzymatically labeled antibody with a substrate.

FIG. 12 is an H filter and a T reactor for use in combination with an H reactor, illustrated with a sandwich immunoassay with subsequent selection of the uncomplexed antibody, followed by reaction of an enzymatically labeled antibody with a substrate.

15 FIG. 13 is an H reactor and subsequent T reactor with diffusion in the plane perpendicular to the channel cell surface, illustrated with a competitive immunoassay and subsequent reaction of an enzymatically labeled antigen with a substrate.

DETAILED DESCRIPTION OF THE INVENTION

20 This invention relates to the following co-pending Patent Applications, all of which are incorporated by reference in their entirety: U.S. Serial No. 08/625,808, "Microfabricated Diffusion-Based Chemical Sensor," filed March 29, 1996, now allowed; U.S. Serial No. 08/829,679, "Microfabricated Diffusion-Based Chemical Sensor," filed March 31, 1997; U.S. Patent Application Serial No. 08/900,926, "Simultaneous Analyte Determination and Reference

Balancing in Reference T-Sensor Devices," filed July 25, 1997; U.S. Serial No. 08/621,170
"Fluorescent Reporter Beads for Fluid Analysis," filed March 20, 1996; U.S. Serial No.
08/663,916, "Microfabricated Differential Extraction Device and Method," filed June 14, 1996;
U.S. Serial No. 08/534,515, "Silicon Microchannel Optical Flow Cytometer," filed September
5 27, 1995; PCT No. 96/15566 "Silicon Microchannel Optical Flow Cytometer," filed September
27, 1996; U.S. Serial No. 08/823,747, "Device and Method For 3-Dimensional Alignment of
Particles in Microfabricated Flow Channels," filed March 26, 1997; U.S. Serial No. 08/876,038,
"Adsorption-Enhanced Differential Extraction Device," filed June 13, 1997; U.S. Serial No.
60/049,533, "Method For Determining Concentration of a Laminar Sample Stream," filed June
10 13, 1997; U.S. Serial No. 08/938,584, "Device for Rapidly Joining and Splitting Fluid Layers,"
filed concurrently herewith; Serial No. 08/938,093, "Multiple Analyte Diffusion Based
Chemical Sensor," filed concurrently herewith.

The channel cells and method of this invention are designed to be carried out such that
all flow is laminar. In general, this is achieved in a device comprising microchannels of a size
15 such that the Reynolds number for flow within the channel is below about 1, preferably below
about 0.1. Reynolds number is the ratio of inertia to viscosity. Low Reynolds number means
that inertia is essentially negligible, turbulence is essentially negligible, and the flow of the two
adjacent streams is laminar, i.e. the streams do not mix except for the diffusion of particles as
described above. Flow can be laminar with Reynolds number greater than 1. However, such
20 systems are prone to developing turbulence when the flow pattern is disturbed, e.g., when the
flow speed of a stream is changed, or when the viscosity of a stream is changed. The preferred
embodiments of this invention utilize liquid streams, although the methods and devices are also
suitable for use with gaseous streams.

The H reactor of this invention is illustrated in plan view in FIG. 1a and in cross section
25 in FIG. 1b. The channel cell containing the H reactor comprises substrate plate 1 and coverplate
2. Sample (primary) stream 11 enters sample stream inlet channel 10 through inlet 3. The
sample contains analyte (small primary) particles 12 and larger particles 13. The term "particles"
refers to any species, including dissolved and particulate species such as molecules, cells,
suspended and dissolved particles, ions and atoms. In this example the sample is whole blood,
30 the analyte is an antigen, and the larger particles are blood cells. Reagent stream 21, also labeled

R1, separately enters reagent stream inlet channel 20 through inlet 4. The term "separately" is used for streams having individual rather than shared flow channels. In this example the reagent particles are antibody 23 bound with labeled antigen 22.

5 The sample and reagent streams join in reaction channel 30 where they flow in adjacent laminar streams, also called companion streams. The term "adjacent" is used herein for both side by side streams, as in FIG. 1, and layered streams, as in FIG. 13. The sample stream enters one side of the reaction channel and the reagent stream enters the other side. The term "side" as used herein refers to both left and right, as in channel 30 of FIG. 1, and top and bottom, as in channel 30 of FIG. 13.

10 Because the flow in the reaction channel is laminar, there is no turbulent mixing of the streams. However, by diffusional mixing the small analyte particles diffuse into the reagent stream and react with the reagent particles to form product particles. The diffusion direction is termed the depth, labeled d , and the orthogonal dimension is termed the width, labeled w . In this example, the native and labeled antigen compete for binding sites on the antibody. By the end
15 of the reaction channel, the reagent stream has become a first product stream, P1, and the sample stream is a residual sample stream. The residual sample stream 41 exits through residual sample stream outlet channel 40 and outlet 5, and product stream 51 flows into product stream channel 50.

20 In the illustrated embodiment the reaction in channel 30 is a complex formation between antigen and antibody. The term "reaction" as used herein includes any interaction between the analyte particle and reagent particle which leads to a detectable change. It includes chemical reaction, physical binding, adsorption, absorption (for example when the analyte particle is sucked inside a porous reagent particle such as a zeolite), antibody reaction, nucleic acid binding, ion pairing, ion exchange, chromatographic type reaction and receptor hormone reaction.

25 The product stream flows into a product particle detection channel. The term product particles refers to all particles in the product stream. They can be, for example, new species formed from reaction, or reagent particles the concentration of which depends on the extent of reaction with analytes. In the example of FIG.1, the displaced labeled antigen and the antibody

with native antigen are both product particles. The detection channel of this invention may be coupled to external detecting means for detecting changes in the reagent particles carried within the product stream as a result of contact with analyte particles. Detection and analysis is done by any means known to the art, including optical means, such as absorption spectroscopy, luminescence or fluorescence, by chemical indicators which change color or other properties when exposed to the analyte, by immunological means, electrical means, e.g. electrodes inserted into the device, electrochemical means, radioactive means, or virtually any microanalytical technique known to the art including magnetic resonance techniques, or other means known to the art to detect the presence of an analyte such as an ion, molecule, polymer, virus, DNA sequence, antigen, microorganism or other factor. Field effects which are ion or chemical sensitive can be measured in the detection channel. Preferably optical means are used, and antibodies, DNA sequences and the like are attached to optical markers. Examples of detection channels are discussed below, following description of further embodiments of the H reactor.

A different reaction scheme is illustrated in FIG. 2. Analyte 14 is an antigen. Reagent stream 21 contains two types of reagent particles, primary antibody 26 and labeled secondary antibody 27. Both antibodies react with the antigen to form product particles, which exit through product channel 50. The secondary antibody can be, for example, fluorescently, luminescently or enzymatically labeled. The first antibody can be sufficiently large that it reduces the diffusion coefficient of the complex enough to diffusionally distinguish between the complexed and uncomplexed labeled antibody.

The reagent particles can be reporter particles immobilized on beads to form reporter beads 24, as shown in FIG. 3. Each reporter bead comprises a bead having a plurality of at least one type of reporter molecules immobilized thereon. A property of the reporter bead, such as fluorescence, luminescence, absorbance or chemical activity, is sensitive to a corresponding analyte. The use of reporter beads allows for a plurality of analytes to be measured simultaneously through a single reagent inlet because the beads can be tagged with different reporter molecules. The reporter bead is illustrated herein with the competitive immunoassay. It could also be used with a sandwich immunoassay or with other reporter molecules.

The reagent particles can be magnetic reporter beads 25, as shown in FIG. 4. Within reaction channel 30, transient magnetic field 35 pulls the beads into the sample stream for reaction with the analyte. The field is then reversed to pull the beads back to the product stream for analysis.

5 Following the H reactor, the product stream flows into a detection channel. Although many detection means can be used, optical detection is preferred. The detection channel can be probed with absorbance, luminescence or fluorescence measurement. The absorbance of the reagent particle can change upon reaction and the detection channel can be monitored in transmission. For this embodiment, the channel cell is made of an optically transparent material
10 such as glass or plastic. The external optical apparatus can be very simple. The sensor can be illuminated on one side with a light source such as a light bulb and diffuser, and the absorbance can be detected on the other side with a camera. Alternatively the fluorescence of reagent particles can change in response to the analyte, in which case the fluorescence can be monitored. Alternatively, the reaction product can be luminescent. For reflection measurements the back
15 side of the channel cell need not be transparent and is preferably made of a reflective material such as silicon.

 For optical detection, the signal can be increased by using convoluted detection channel, as shown in FIG. 5. A product stream, P, enters the detection channel. There is a difference in optical properties between bound antigen 22a and unbound antigen 22b. It can be a difference
20 in, for example, color, fluorescence intensity, or degree of polarization of the fluorescence. In this embodiment, detection channel 100 includes a series of turns, making a square wave geometry. The flow channel can be convoluted in any of a number of ways. In another embodiment, the flow channel is in the shape of a coil. In lieu of a convoluted channel, the channel can include a broadened region, as shown in detection channel 110 of FIG. 6. An
25 external light source and photodetector are positioned about the detection channel for absorbance or fluorescence measurements. Only a photodetector is required for luminescence.

 In the embodiment of FIG. 7, the optical measurement is facilitated by diffusional separation of the unbound antigen. The product stream enters detection channel system 120 through product stream channel 121 which, if there are no intervening elements, is product

stream channel 50 of the H reactor. Extraction fluid stream 124 enters through extraction stream inlet 122. The extraction fluid can be any fluid capable of accepting particles diffusing from the product stream. Preferred extraction streams comprise water and isotonic solutions such as salt water or organic solvents like acetone, isopropyl alcohol, ethanol, or any other convenient liquid which does not interfere with the product particles or the detection means. The streams join in adjacent laminar flow in joining channel 123. Both separation and detection take place in the joining channel. Free antigen 22b diffuses more rapidly than bound antigen 22a. To select between the bound and unbound antigen, photo illumination or detection is focused on one side of channel 123.

Another embodiment of optical detection uses single particle detection, for example as in flow cytometer detection channel 130, shown in FIG. 8. The product stream contains particles which are formed into a single file for the flow cytometer. This is particularly suitable for product streams containing reporter beads 24. As illustrated, the smaller particles are not necessarily single file. One embodiment of the flow cytometer uses a v-groove flow channel. The v-groove channel is described in detail in U.S. Patent Application 08/534,515, filed September 27, 1995, which is incorporated by reference herein in its entirety. The cross-section of such a channel is like a letter V, and thus is referred to as a v-groove channel. The v-groove preferably has a width small enough to force the particles into single file, but large enough to pass the largest particles without clogging. An optical head comprising a laser and small and large angle photodetectors adapted for use with a v-groove flow channel can be employed.

An alternative means of achieving single file particle flow through a flow channel is the sheath flow module disclosed in U.S. Patent Application 08/823,747, filed March 26, 1997 and incorporated in its entirety by reference herein. The sheath flow module includes sheath fluid inlets before and after, and wider than, a sample inlet. The product stream is surrounded by sheath fluid, and the sheathed stream is focused to produce single file particles.

In dual detection embodiments of the invention, residual sample stream 41 is coupled with a flow cytometer. Alternatively, the fluid stream can flow first through a flow cytometer and then through the H reactor. This allows independent detection of both the smaller and larger analyte particles, for example both undissolved and dissolved analytes or both antigens and cells.

The channel cell of this invention can be used to introduce two reagent streams, a first reagent stream in the H reactor and a second reagent stream in either a T reactor or a second H reactor. For example, in a sandwich immunoassay primary and secondary antibodies can be separately introduced, as shown in FIG. 9. The H reactor comprises sample stream inlet channel 10, first reagent stream inlet channel 20, reaction channel 30, residual sample stream outlet channel 40 and product stream channel 50. The first reagent stream contains primary antibody 26, which reacts with antigen in the sample to form a first product stream, P1.

A second reagent is introduced to the first product in reagent stream 61 (R2) through second reagent stream inlet channel 60. The second reagent stream contains labeled secondary antibodies 27. The first product stream and second reagent stream flow in adjacent laminar streams in joining channel 70, which functions as a reaction channel. In this illustration, the reaction channel is sufficiently long to allow both the first product particles and the second reagent particles to diffuse to the adjacent stream. In one embodiment, the first or second reagent particles are immobilized on magnetic beads and a magnetic field is used to pull the beads to one side of channel 70 for reaction. The beads can remain on that side or be pulled to the other side with a reversed field.

A second product stream, P2, exits in stream 71 through channel 70. Having first and second reagent inlets can be useful, for example, to allow undesirable side reactions to go to completion before the addition of the second reagent. Particles diffuse between the first product and second reagent streams to form a second product. The second product stream 71 then enters a detection channel, for example an optical detection channel as illustrated in FIGS. 5-8.

In generic terms, stream 61 is a companion stream to the first product stream. After diffusion of small particles between the companion stream and the first product stream, which takes place in second laminar flow channel 70, the streams are termed diffused first product and diffused companion streams.

Another application of a second reagent channel is for chemical detection of product particles. In the above examples, the reagent particles are fluorescently labeled. They can alternatively be chemically labeled, for example enzymatically labeled. In the embodiment of

FIG. 10, the antigen in the first reagent is enzymatically labeled. The first product stream flows out of the H reactor (not shown) in product stream channel 50. It contains some bound antigen 22a and some unbound antigen 22b which has been displaced from the antibody by the native antigen from the sample. The enzymatic activity is different in the bound and unbound antigen, typically the unbound antigen is more active. Enzyme substrate particles 62 in second reagent stream 61 enter through second reagent stream inlet channel 60. In joining (reaction) channel 70 they react with the labeled antigen to produce enzyme product particles 72. Second reaction stream 71 flows into a detection channel to detect the enzyme product optically or otherwise. From the amount of enzyme product detected, the amount of antigen in the sample stream can be calculated.

In yet another embodiment, reagent particles 62 react with a first product particle to form a chemiluminescent or bioluminescent product. The luminescence is optically detected. Chemiluminescent reagents are readily available (see, for example, "Tropix Luminescence Products", 1997, Perkin Elmer Applied Biosystems, Bedford, Massachusetts). Luminescent reagents can also be bound to antibodies and antigens to make luminescently labeled reagent particles.

In a sandwich immunoassay the secondary antibody can likewise be enzymatically labeled as shown in FIGS 11-12. These embodiments further illustrate an H separator between the H reactor and the T reactor. First product stream P1 leaves the H reactor (not shown) through first product stream channel 50. In the illustrated embodiment one type of product particles is a sandwich of native antigen between primary antibody 26 and enzymatically labeled secondary antibody 27a. The sandwich product particles can be formed in a single step, as in FIG. 2, or in two steps, as in FIG. 9. The product stream contains both bound labeled antibodies 27a and unbound labeled antibodies 27b. Rather than distinguish them based on relative chemical activity, they can be separated by diffusion prior to the second reaction.

These embodiments include an H separator. The product stream enters through channel 50 and a companion stream, extraction stream 81, enters through extraction stream inlet 80. The two streams flow in adjacent laminar streams in separation channel 85. The smaller product particles, in this case the unbound antibodies, diffuse into the extraction stream faster than the

sandwich complex. The two product streams, the residual first product stream P1' containing the larger particles and the diffused first product stream P1" containing the smaller particles, are separated into channels 92 and 90, respectively.

5 In the embodiment of FIG. 11 the larger particles enter a T reactor. In reaction channel 70, the product stream flows adjacent to a companion stream, the second reagent stream, which enters through inlet channel 60. Enzyme substrate 62 is converted into enzyme product 72, which flows out in product stream P2 for subsequent detection. In the embodiment of FIG. 12, the lighter product stream in channel 90 meets the second reagent stream, which enters through
10 channel 60, in reaction channel 70. Again the enzyme substrate is converted to enzyme product, which is subsequently detected.

In addition to the product stream outlets illustrated above, additional outlets can be provided for conducting specimen streams from the product stream channel, or at successive intervals along the length of the reaction channel. The specimen channels can be, for example,
15 smaller channels branching from the reaction or product channels. Analyte concentration can be measured in the specimen streams by means such as viewports, fluorescence detectors or flow cytometers.

The length of the reaction channels and the distance traveled by the product stream prior to detection can be selected to allow reactions to go to completion, to limit the sampling of
20 constituents based on their diffusion constants, and to alter the efficiency of separation of particles. The reaction channel is long enough to permit small analyte particles to diffuse from the sample stream and have a detectable effect on reagent particles, preferably at least about 2 mm long. The diffusion time required depends on the diffusion coefficient of the analyte particles. The reaction time required depends on the reaction rate. Some reactions, such as ion
25 reactions, are completed within microseconds. Some reactions, such as competitive immunoassays that involve unloading a bound antigen, require minutes. To allow greater time for reaction between the analyte particles and the reagent particles, the length of the product stream channel can be increased.

The length of the flow channel depends on its geometry. The flow channel can be straight or convoluted. Convoluted channels provide longer distances for diffusion or reaction to occur without increasing the size of the substrate plate in which the channel is formed, thereby allowing for measurement of analytes with smaller diffusion coefficients or reaction rates. The diffusion coefficient of the analyte, which is usually inversely proportional to the size of the analyte, affects the desired reaction channel length. For a given flow speed, particles with smaller diffusion coefficients require a longer flow channel to have time to diffuse into the reagent stream. In preferred embodiments of this invention the channel length of a straight reaction channel is between about 5 mm and about 50 mm. In embodiments of this invention wherein the reaction channel is convoluted, the length of the channel is defined or limited only by the size of the microchip or other material into which the channel is etched or otherwise formed.

As an alternative to increasing channel length to allow more diffusion or reaction of analyte particles, the flow rate can be decreased or the flow may be stopped to allow reactions to proceed and then restarted. However, several factors limit the minimum flow rate. First, the flow rate is typically achieved by a pumping means and some types of pumps cannot produce as low a pressure and flow rate as may be desired to allow enough time for diffusion of the particles. Second, if the flow rate is too slow, particles more dense than the surrounding fluid may sink to the bottom of the flow channel and particles less dense than the surrounding fluid may float to the top of the flow channel. It is preferable that the flow rate be fast enough that hydrodynamic forces substantially prevent particles from sinking to the bottom, floating to the top, or sticking to the walls of the flow channel. In some applications, notably use in space, sedimentation is not a factor. Sedimentation can be avoided by orienting the channel cell with the laminar flow reaction channel vertical.

The flow rate of the input streams is preferably between about 5 micrometers/second and about 5000 micrometers/second, more preferably about 25 micrometers/second. Preferably the flow rate for both the sample and reagent streams is the same.

By adjusting the configuration of the channels in accordance with the principles discussed above to provide an appropriate channel length, flow velocity and contact time between the

sample stream and the reagent stream, the size of the particles remaining in the sample stream and the particles diffusing into the reagent stream can be controlled. The contact time required can be calculated as a function of the diffusion coefficient of the particle and the distance over which the particle must diffuse. If the diffusion coefficient of the larger particles is about ten times smaller than the coefficient for the analytes, the product stream should be substantially free of the large particles.

The channel cell of this invention has been demonstrated with diffusional separation occurring in a plane parallel to the channel cell surface, termed the parallel embodiment. The channels can alternatively be formed so that the diffusional separation takes place in a plane orthogonal to the channel cell surface. Figure 13 is a cross section of an H reactor and a T reactor formed in the orthogonal plane, termed the orthogonal embodiment. The channels are formed between substrate plate 1 and coverplate 2. The H reactor is formed by sample (primary) stream inlet channel 10, first reagent stream inlet channel 20, reaction channel 30, residual sample stream outlet channel 40 and first product stream channel 50. The first reagent stream inlet can, like the sample inlet, feed through the substrate plate.

As in the parallel configuration, the diffusion direction is termed the depth, labeled d , but note that the diffusion direction, and hence the depth, in FIG. 13 is orthogonal to the diffusion direction in FIG. 1. The depth of channel 30 is optionally greater than the depth of channels 20 and 50 to accommodate two streams. Although this H reactor does not have the visual appearance of the letter "H", it has the functional criteria of two laminar flow channels joining in the upstream end of a reaction channel to form adjacent flow streams, layered in this case rather than side by side, and two laminar flow channels branching from the downstream end of the reaction channel.

The product stream of the H reactor of FIG. 13 enters a T reactor comprising product stream channel 50, second reagent stream inlet channel 60, and reaction channel 70. The depth of channel 70 is optionally greater than the depth of channel 50 to accommodate two streams. In the previous embodiments (see FIG. 9, for example), channels 50 and 60 were collinear; in this embodiment they join at a right angle. As in the case of the H reactor, it is not the visual appearance of the letter "T" that defines the T reactor, but rather the functional criteria of the

product stream channel joining a companion stream inlet channel to form adjacent laminar streams in the reaction channel.

5 The perpendicular embodiment can have a larger contact area between the sample and reagent streams than the parallel version. The width of the flow channel in the perpendicular embodiment can be increased to increase the contact area while maintaining laminar flow. This allows a greater reaction volume, which is particularly advantageous for the synthesis application of the device. The parallel embodiment is cheaper and easier to fabricate, which is particularly advantageous in the analysis application of the device.

10 In either the parallel or perpendicular embodiment, the channel cell is generally formed by two plates with abutting surfaces. The channels may be formed in both plates, or one plate can contain the channels and the other can be a flat cover plate. The channel cells of this invention may be formed by any techniques known to the art. Silicon channel plates are preferably formed by etching the flow channels onto the horizontal surface of a silicon microchip and placing a cover plate, preferably of an optically clear material such as glass or a silicone
15 rubber sheet, on the etched substrate plate. To promote flow, the corners can be etched. For non-silicon channel plates, other means for manufacturing the channel cells of this invention include molding the device in plastic, micromachining, and other techniques known to the art. Precision injection molded plastics can also be used to form the devices. In a preferred embodiment of this invention, channel cells have hydrophilic surfaces to facilitate flow of liquid
20 therein and allow operation of the device without the necessity for pressurization. The substrate may be treated by means known to the art following fabrication of the channels to render it hydrophilic. The cover plate is also preferably treated to render it hydrophilic.

25 For optical detection in transmission, such as absorbance detection, the analyte detection area, and optionally other parts of the channel cell system, are optically accessible. Typically the detection area lies between optically transparent plates. Analyte detection area as used herein refers to that portion of a flow channel where changes in the analyte particles or the reagent particles are measured. For detection with reflection, such as fluorescence or luminescence detection, only one plate need be transparent, typically the cover plate. For product synthesis, the channel system need not be transparent in any portion.

The preferred channel dimensions depend on the application, with the criterion that laminar flow must be maintained. The channel depth (diffusion direction) is preferably between about 10 and 1000 μm , and most preferably around 400 μm , in both the parallel and perpendicular embodiments. The channel width is about 10-200 μm in the parallel embodiment. In the perpendicular embodiment, it can be more than several millimeters wide and still maintain laminar flow.

Means for applying pressure to the flow of the feed fluids through the device can also be provided. Such means can be provided at the inlets and/or the outlets (e.g. as vacuum exerted by chemical or mechanical means). Means for applying such pressure are known to the art, and include the use of a column of water or other means of applying water pressure, electroosmotic forces, optical forces, gravitational forces, and surface tension forces. The outlets can be connected to fluid receptacles. Such receptacles may be coupled to an analytical or detection device.

Various aspects of this invention have been illustrated with specific examples. Combinations and variations of these embodiments will be readily apparent to those skilled in the art and fall within the spirit and scope of this invention. For example, any of the exemplified configurations and reaction schemes can be implemented with reagent particles immobilized on beads. The beads can be magnetic and magnetic fields can be used to manipulate the beads. Filters, diffusion based or otherwise, can be placed before or after the H reactor, and can be positioned between the H reactor and subsequent reactors, separators and detectors. Each reagent stream can contain more than one type of reagent particle for detection of a single type of analyte particle or for simultaneous detection of multiple analytes. More than one reagent stream channel can join the upstream end of the reaction channel, or more than one reagent stream channel can merge prior to joining the reaction channel. More than one product stream channel can leave the downstream end of the reaction channel. In addition to detecting species in the product stream, the residual sample stream and any of the companion streams can be analyzed. The angles of the "H" and "T" are not limited to right angles. Parallel and perpendicular geometries can be combined in one channel system. This reactor can be used in combination with other sample preparation and analysis apparatus.

Example 1

Tests performed by EMIT (Enzyme Multiplied Immunoassay Technique) can be carried out in the H reactor combined with the T reactor of this invention. EMIT is a homogeneous immunoassay for low-molecular-weight ligands. The assay is based on binding of antibody to an enzyme labeled ligand in order to change the enzyme activity. The competitive binding of antibody bound and unbound ligands is used to measure the concentration of unbound ligand. Here, digoxin, a drug used to control cardiac arrhythmias and requiring frequent concentration analysis in case of intoxication, is selected as an example test. The EMIT assay for digoxin is based on the competitive binding between drug in the sample and drug labeled with glucose-6-phosphate dehydrogenase made using recombinant DNA technology (rG6P-DH) for antibody binding sites. The drug concentration is measured through enzyme activity which decreases upon binding to the antibody. Active enzyme reduces NAD to NADH.

The reaction is illustrated in FIG. 1 combined with FIG. 10. In this assay, reagent stream R1 contains digoxin labeled with glucose-6-phosphate dehydrogenase 22 and antibody 23. Reagent stream R1 is imported through channel 20 and contacts the sample stream from channel 10. Digoxin in the sample 12 diffuses into the reagent stream in channel 30, binds with antibody and is transported to channel 50, while cellular components are transported to channel 40. The more digoxin molecules in the sample stream, the more antibody binds with free digoxin instead of enzyme labeled digoxin. As a result, the more enzyme is freed from antibody binding.

In channel 70, the product stream encounters reagent stream R2, containing two types of reagent particles, the substrate glucose-6-phosphate (not shown) and NAD 62. Freed enzyme oxidizes glucose-6-phosphate and reduces NAD to NADH 72. In the second product stream, the residual enzyme activity is measured by spectroscopy through the change in absorbance by NADH at 340 nm.

Example 2

In another embodiment using multiple reagents in series, the sample stream is blood to be analyzed for glucose, the first reagent stream R1 contains glucose oxidase, and the second reagent stream R2 contains a pH sensitive dye. In channel 30 glucose particles from the blood diffuse into the reagent stream and are changed to gluconic acid. In channel 70 the gluconic acid

reacts with the pH-sensitive dye. In the second product stream, the reaction is detected by changes in the dye absorbance.

CLAIMS

We Claim:

1. A method for reacting small primary particles from a primary stream also comprising larger particles, comprising the steps of:

5 conducting said primary stream into a first laminar flow reaction channel;

 separately conducting a first reagent stream comprising first reagent particles into said first reaction channel, such that said primary stream and said first reagent stream flow in adjacent laminar streams;

10 allowing said small primary particles to diffuse from said primary stream into said first reagent stream, and to react with said first reagent particles and form first product particles, thereby converting said first reagent stream into a first product stream and said primary stream into a residual primary stream comprising said larger particles;

 conducting said residual primary stream out of said first reaction channel; and

 separately conducting said first product stream out of said first reaction channel.

15 2. The method claim 1 further comprising the step of detecting said first product particles.

3. The method of claim 2 wherein said step of detecting said first product particles comprises a method selected from the group consisting of optical, electrical, calorimetric and chemical detection.

20 4. The method of claim 2 wherein said step of detecting comprises absorbance, luminescence or fluorescence detection.

5. The method of claim 1 further comprising the steps of:

conducting said first product stream into a second laminar flow channel;

separately conducting a first companion stream into said second laminar flow channel such that said first product stream and said first companion stream flow in adjacent laminar streams; and

5 allowing small particles in said first product stream or said first companion stream to diffuse therebetween, thereby converting said first product stream into a diffused first product stream and said first companion stream into a diffused first companion stream.

6. The method of claim 5 further comprising the steps of conducting said diffused first product stream out of said second laminar flow channel and separately conducting said diffused
10 first companion stream out of said second laminar flow channel.

7. The method of claim 6 further comprising the steps of:

conducting said diffused first product stream into a third laminar flow channel;

separately conducting a second companion stream into said third laminar flow channel; and

15 allowing small particles in said diffused first product stream or said second companion stream to diffuse therebetween.

8. The method of claim 6 further comprising the steps of:

conducting said diffused first companion stream into a third laminar flow channel;

20 separately conducting a second companion stream into said third laminar flow channel; and

allowing small particles in said diffused first companion stream or said second companion stream to diffuse therebetween.

9. The method of claim 5 wherein said first companion stream is an extraction stream and wherein said first product particles diffuse into said extraction stream.

5 10. The method of claim 5 wherein said first companion stream is a second reagent stream comprising second reagent particles and wherein said second reagent particles react with said first product particles to form second product particles.

11. The method of claim 10 further comprising the step of detecting said second product particles.

10 12. The method of claim 1 wherein said first reagent particles are immobilized on beads.

13. The method of claim 12 wherein said beads are magnetic.

14. The method of claim 12 further comprising the step of detecting said first product particles using single particle detection.

15 15. The method of claim 1 further comprising the step of analyzing said residual primary stream.

16. The method of claim 1 wherein said primary stream is blood, said small primary particles are native antigens, and said first reagent particles are first antibodies.

20 17. The method of claim 16 wherein said first antibodies are bound with labeled antigens, and wherein said native antigens and said labeled antigens compete for binding sites on said first antibodies.

18. The method of claim 16 wherein said first reagent stream further includes second antibodies, and wherein said first and second antibodies form a sandwich complex with said native antigens.

19. A microchannel system for reacting small primary particles in a primary stream also comprising larger particles, comprising:

a first laminar flow channel having an upstream end and a downstream end and having first and second sides;

a primary stream inlet channel connected to said first side of said upstream end of said first laminar flow channel;

a first companion stream inlet channel connected to said second side of said upstream end of said first laminar flow channel, whereby said primary stream and said first companion stream flow in adjacent laminar streams;

a residual primary stream outlet channel connected to said first side of said downstream end of said first laminar flow channel;

a first product stream channel, having an upstream end and a downstream end, said upstream end of said product stream channel connected to said second side of said downstream end of said first laminar flow channel;

a second laminar flow channel having an upstream end and a downstream end, and connected at said upstream end to said downstream end of said first product stream channel; and

a second companion stream inlet channel connected to said upstream end of said second laminar flow channel, whereby said first product stream and said second companion stream flow in adjacent laminar streams.

20. The microchannel system of claim 19 further comprising a detection channel connected to said downstream end of said second laminar flow channel.

21. The microchannel system of claim 20 wherein said detection channel is optically accessible.

5 22. The microchannel system of claim 21 wherein said detection channel is convoluted.

23. The microchannel system of claim 20 wherein said detection channel comprises a flow cytometer channel.

24. The microchannel system of claim 23 wherein said flow cytometer channel comprises a sheath flow module.

10 25. The microchannel system of claim 23 wherein said flow cytometer channel is a v-groove.

26. The microchannel system of claim 19 further comprising:

a first outlet stream channel having an upstream end and a downstream end, said upstream end connected to said downstream end of said second laminar flow channel; and

15 a second outlet stream channel connected to said downstream end of said second laminar flow channel.

27. The microchannel system of claim 26 further comprising a detection channel connected to said downstream end of said first outlet stream channel.

28. The microchannel system of claim 26 further comprising:

20 a third laminar flow channel having an upstream end and a downstream end, said upstream end connected to said downstream end of said first outlet stream channel; and

a third companion stream inlet connected to said upstream end of said third laminar flow channel, whereby said first outlet stream and said third companion stream flow in adjacent laminar streams.

29. The microchannel system of claim 19 further comprising:

5 a third laminar flow channel having an upstream end and a downstream end, said upstream end connected to said downstream end of said second laminar flow channel; and

a third companion stream inlet connected to said upstream end of said third laminar flow channel.

10 30. The microchannel system of claim 19 further comprising a third companion stream inlet channel connected to said upstream end of said first laminar flow channel.

31. The microchannel system of claim 19 further comprising a second product stream outlet channel connected to said downstream end of said first laminar flow channel.

15 32. The microchannel system of claim 19 wherein said system is formed with a substrate plate having channels formed therein and a cover plate bonded to said substrate plate.

33. The microchannel system of claim 32 wherein the configuration of said primary stream inlet and first companion stream inlet is such that said primary and first companion streams flow in side by side laminar streams in said first laminar flow channel.

20 34. The microchannel system of claim 32 wherein the configuration of said primary stream inlet and first companion stream inlet is such that said primary and first companion streams flow in layered laminar streams in said first laminar flow channel.

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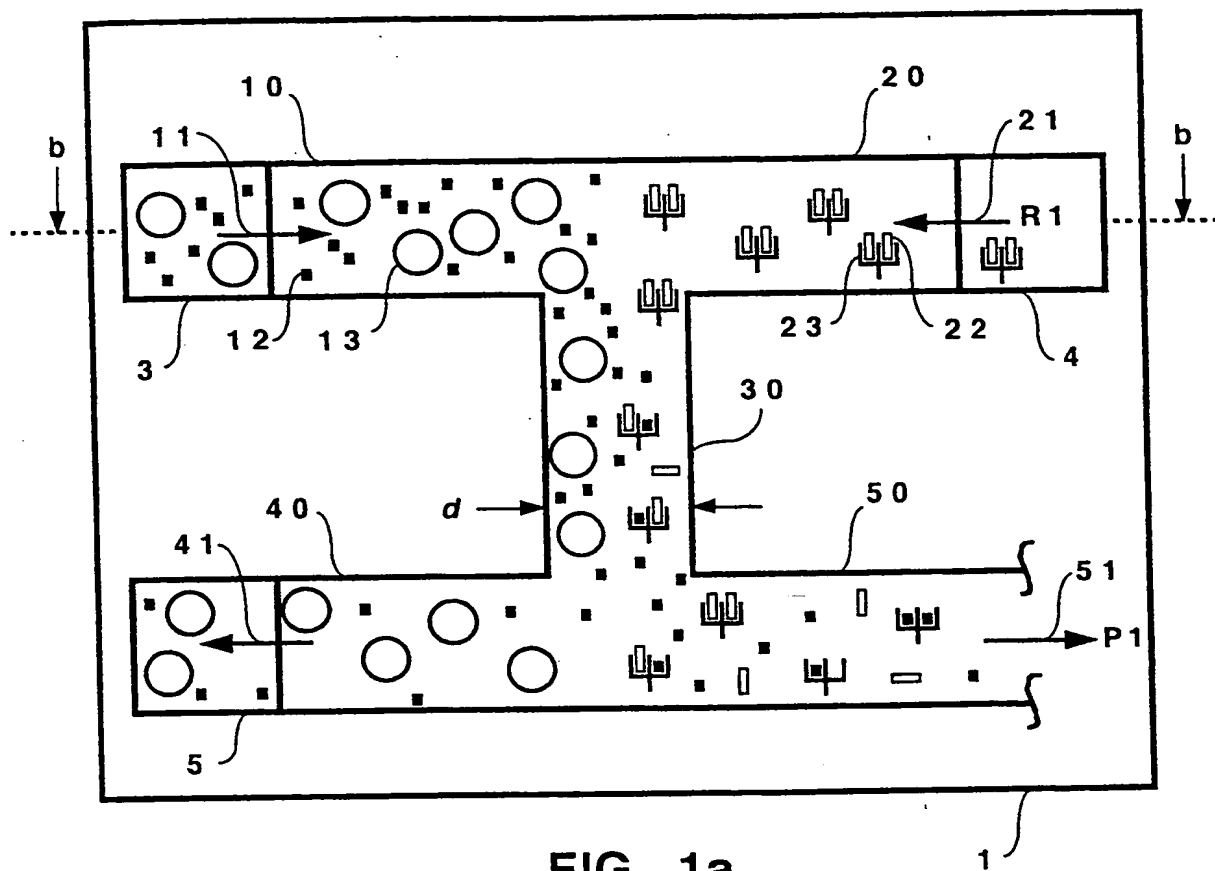


FIG. 1a

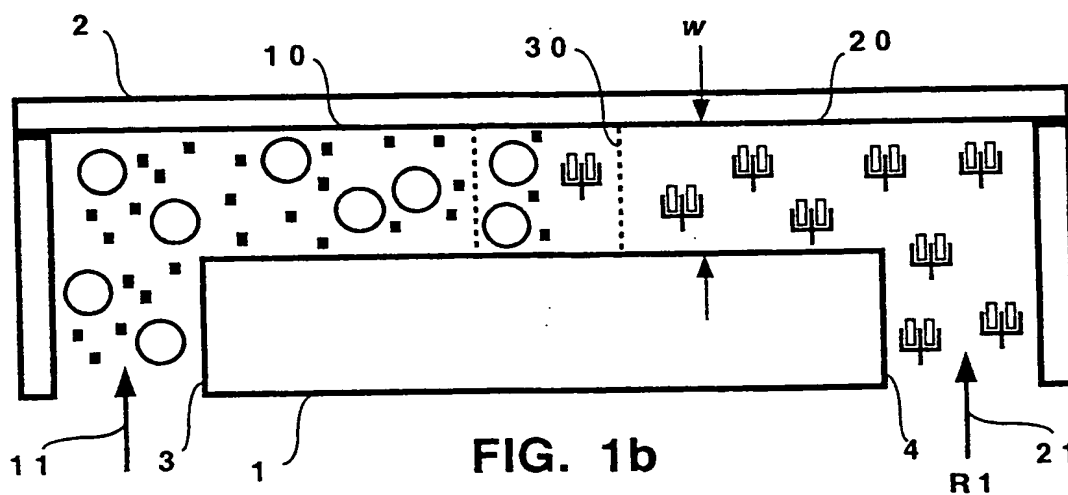


FIG. 1b

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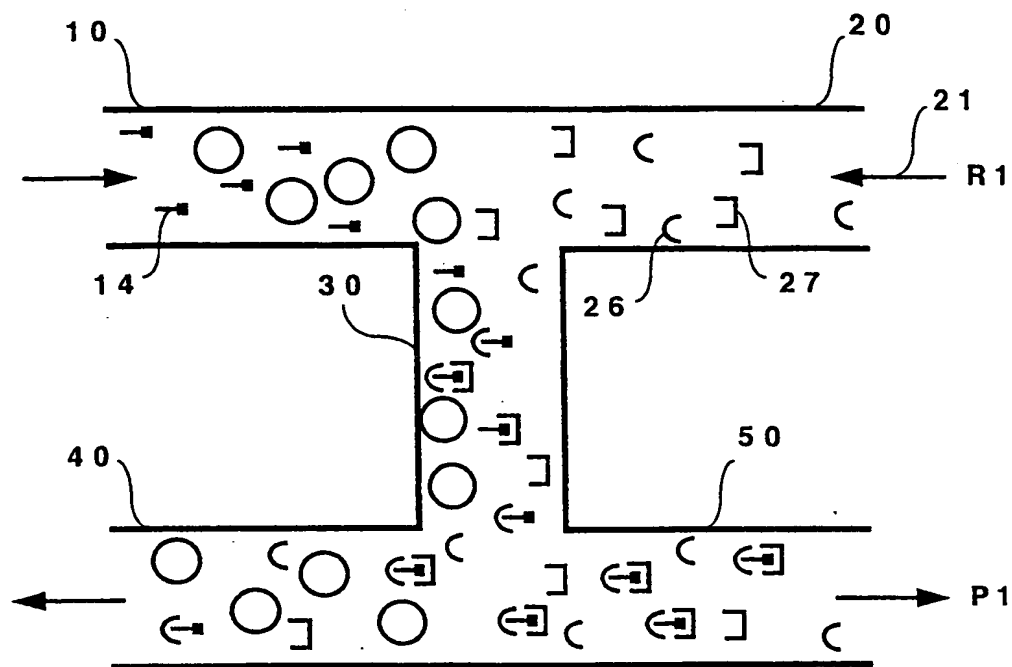


FIG. 2

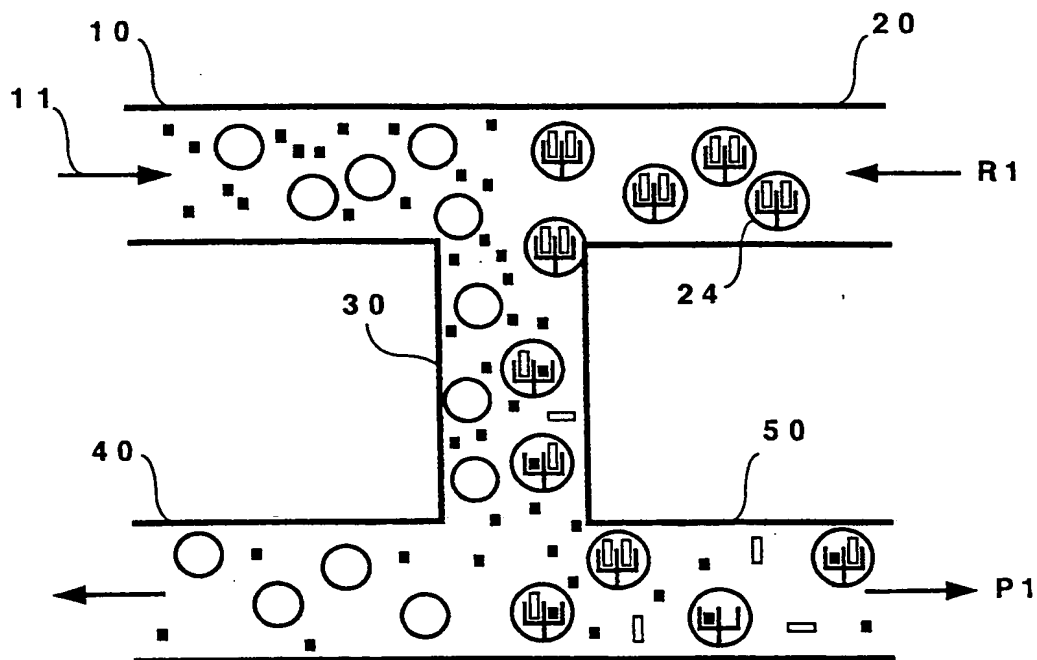


FIG. 3

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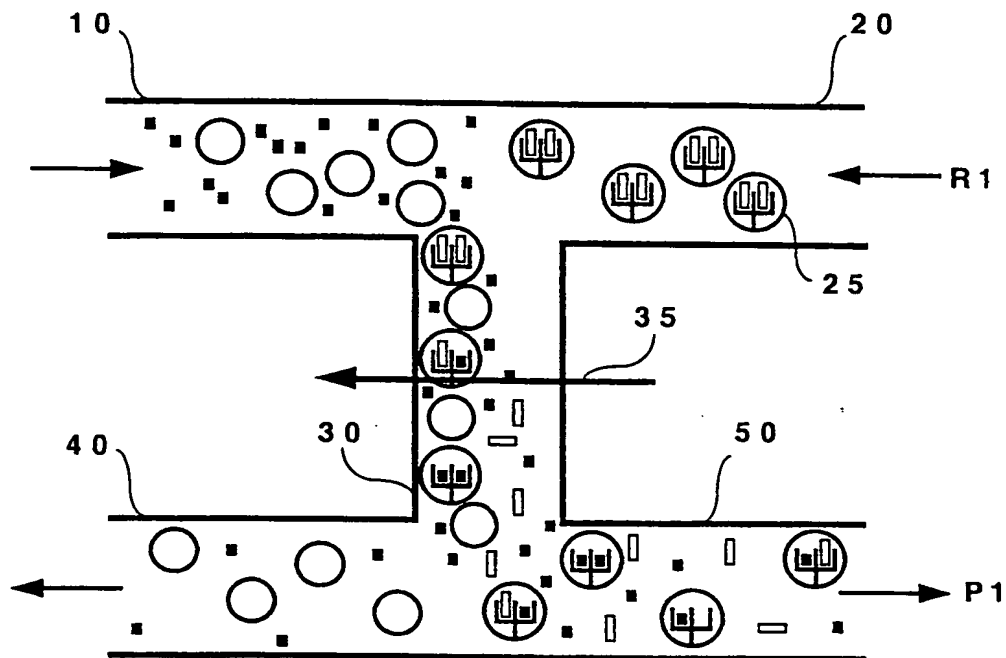


FIG. 4

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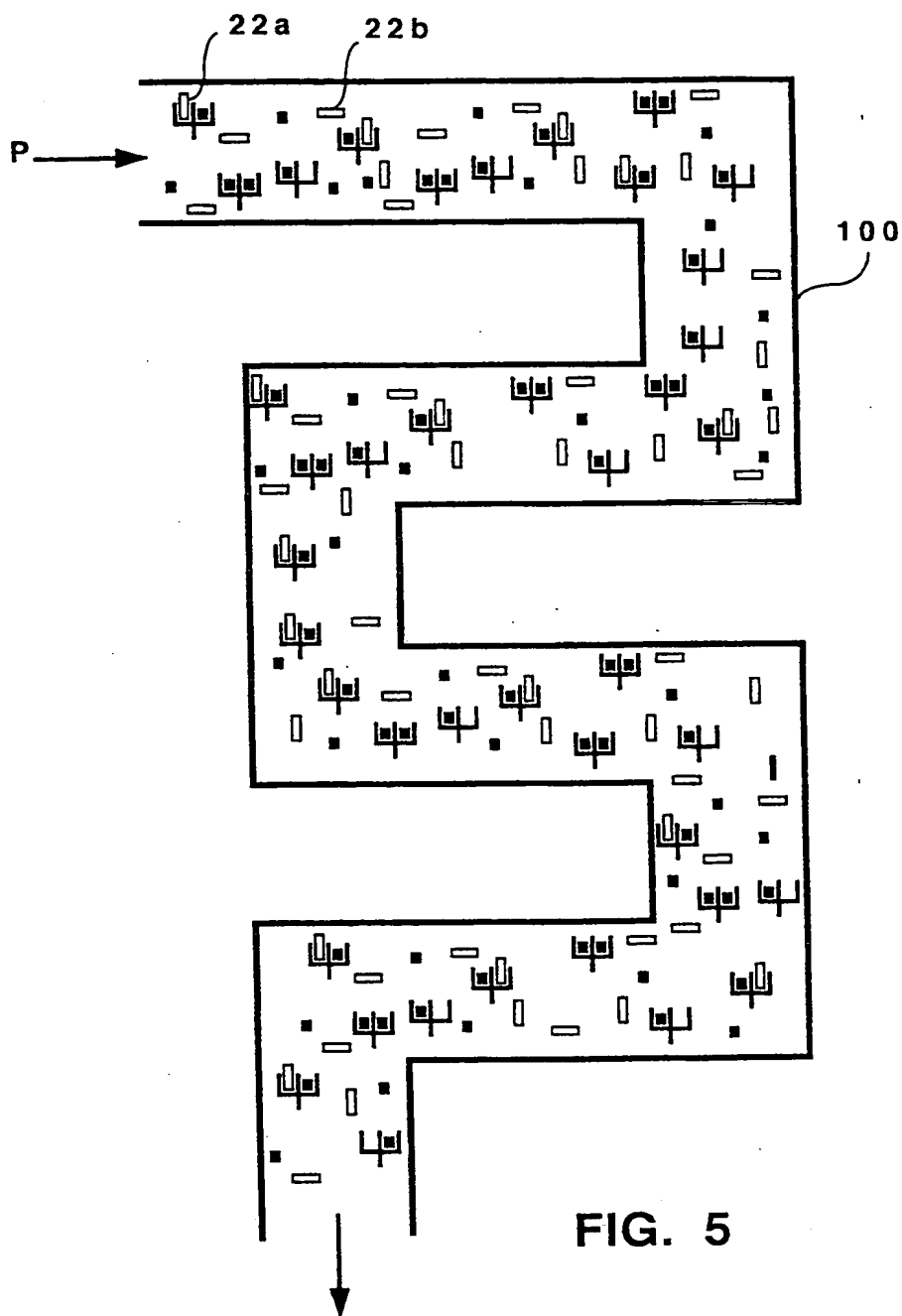


FIG. 5

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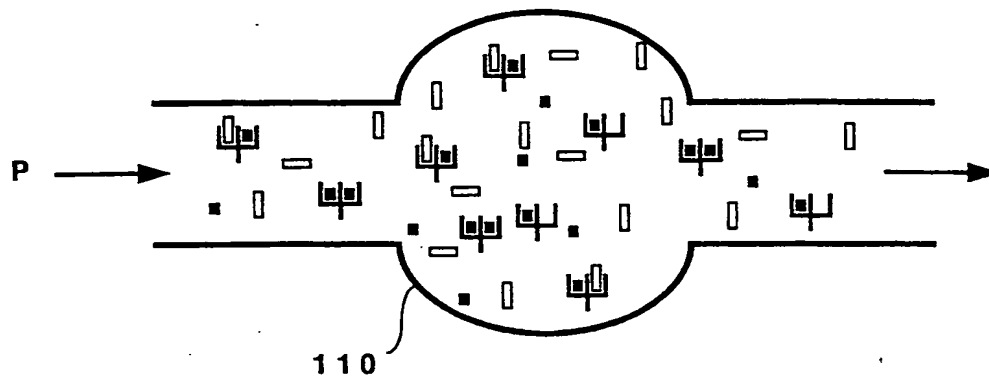


FIG. 6

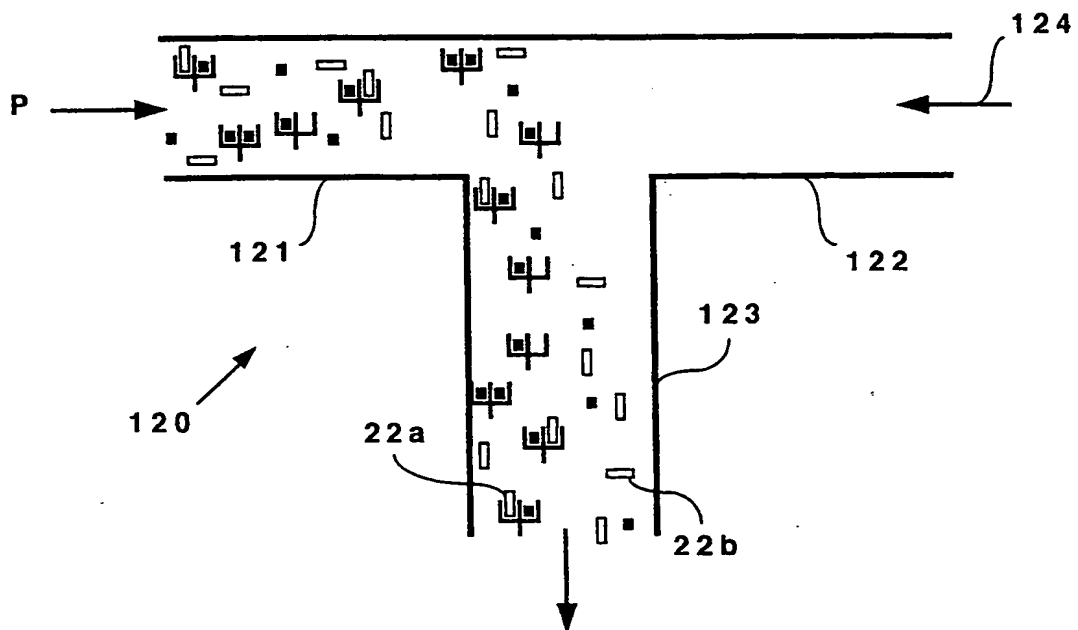


FIG. 7

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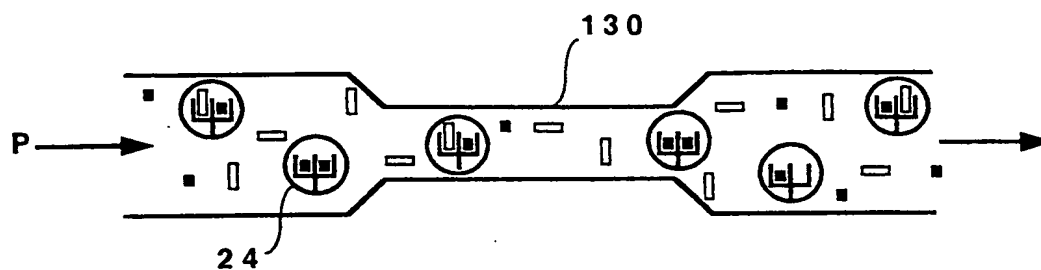


FIG. 8

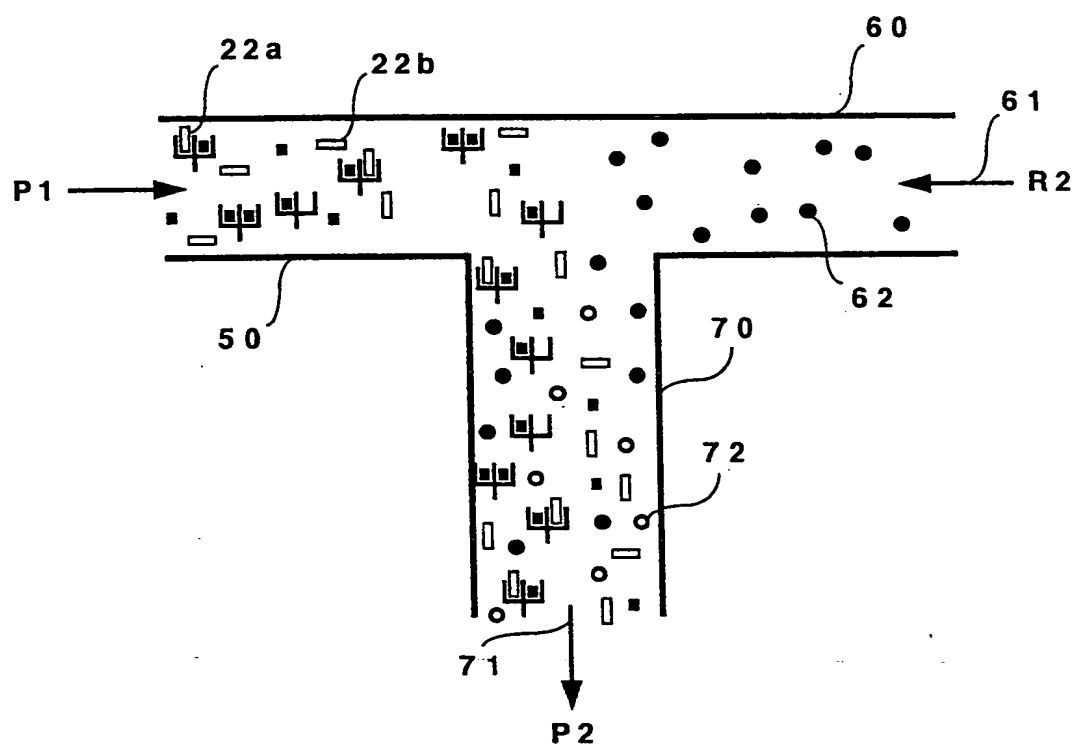


FIG. 10

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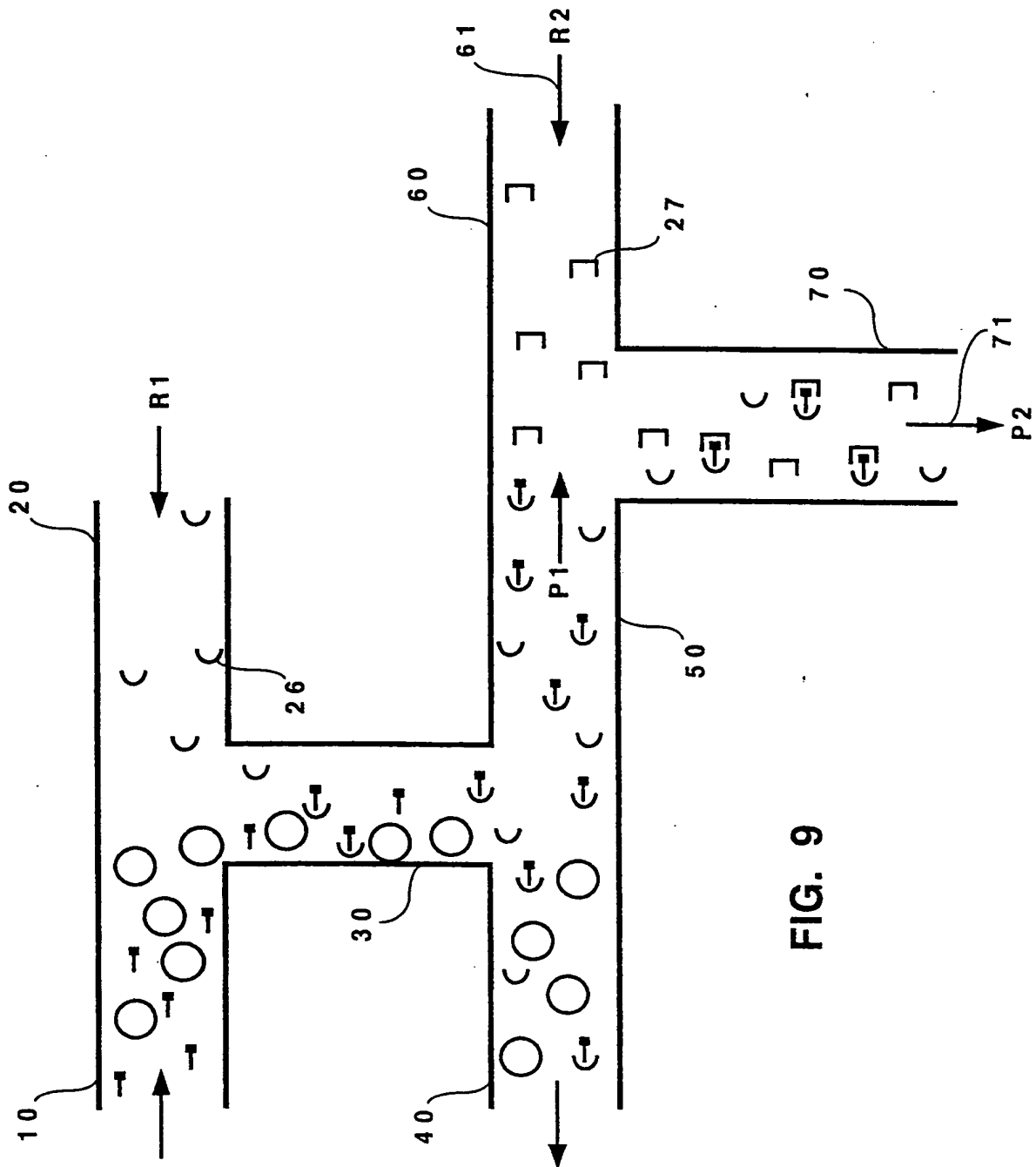


FIG. 9

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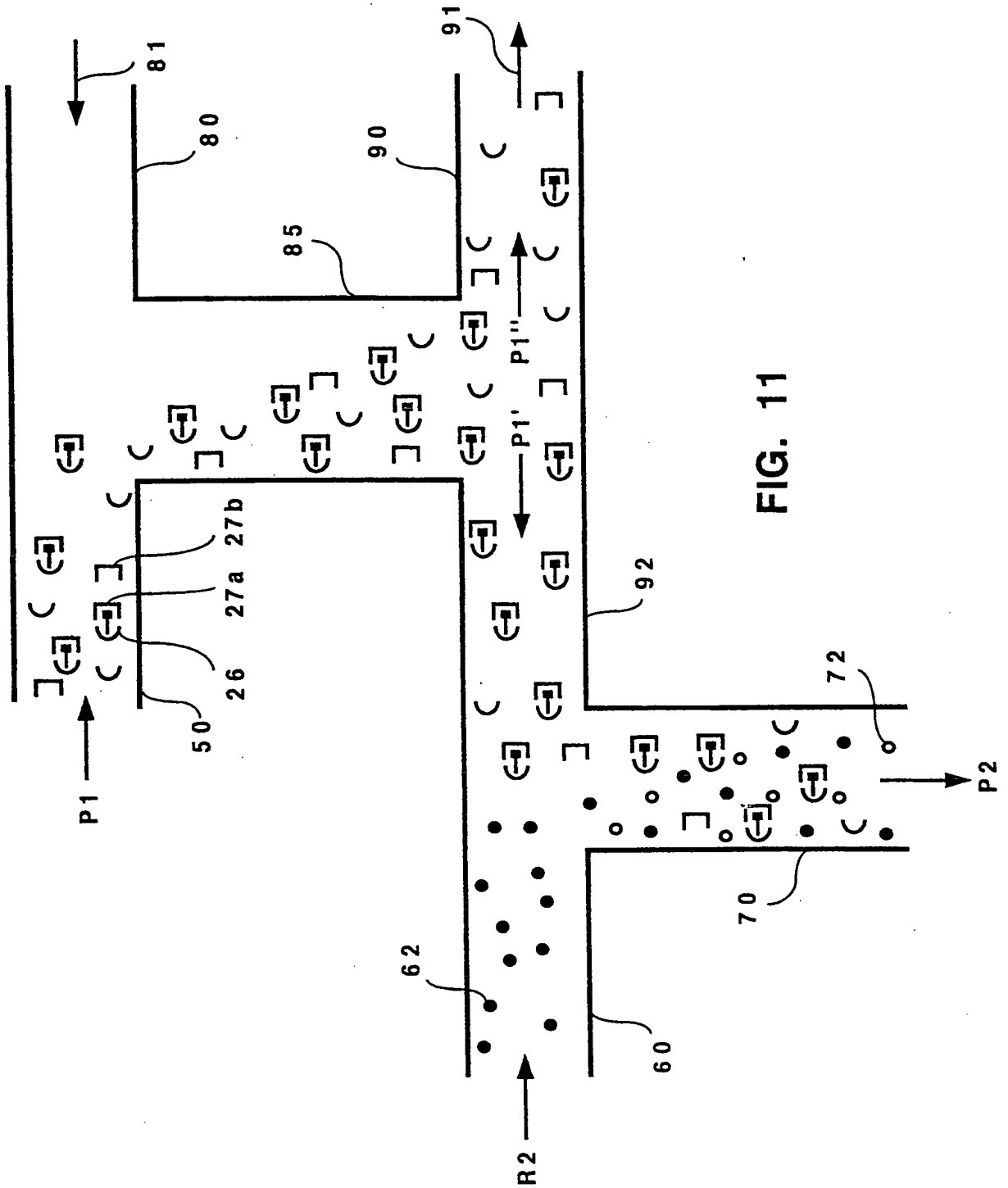


FIG. 11

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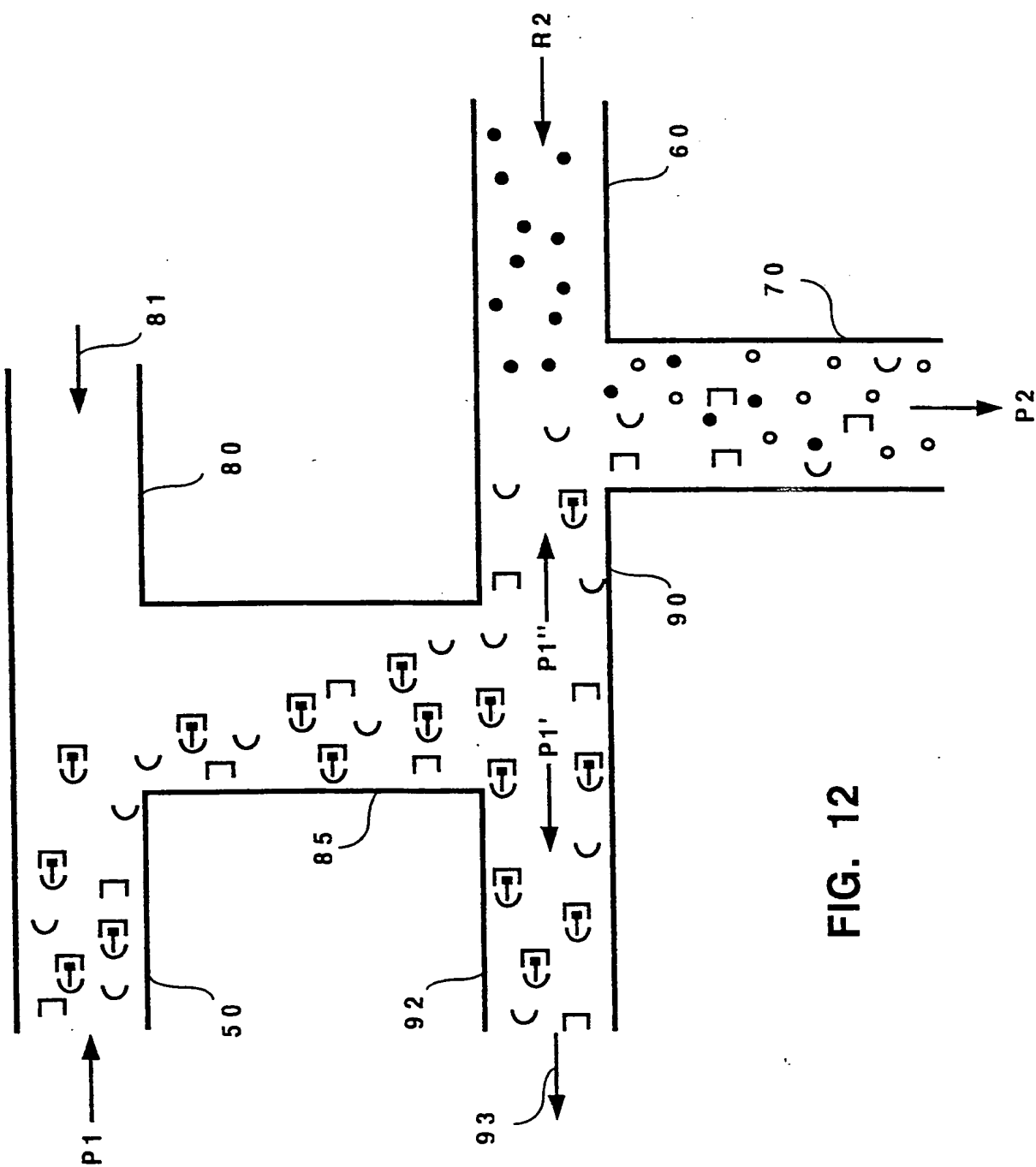


FIG. 12

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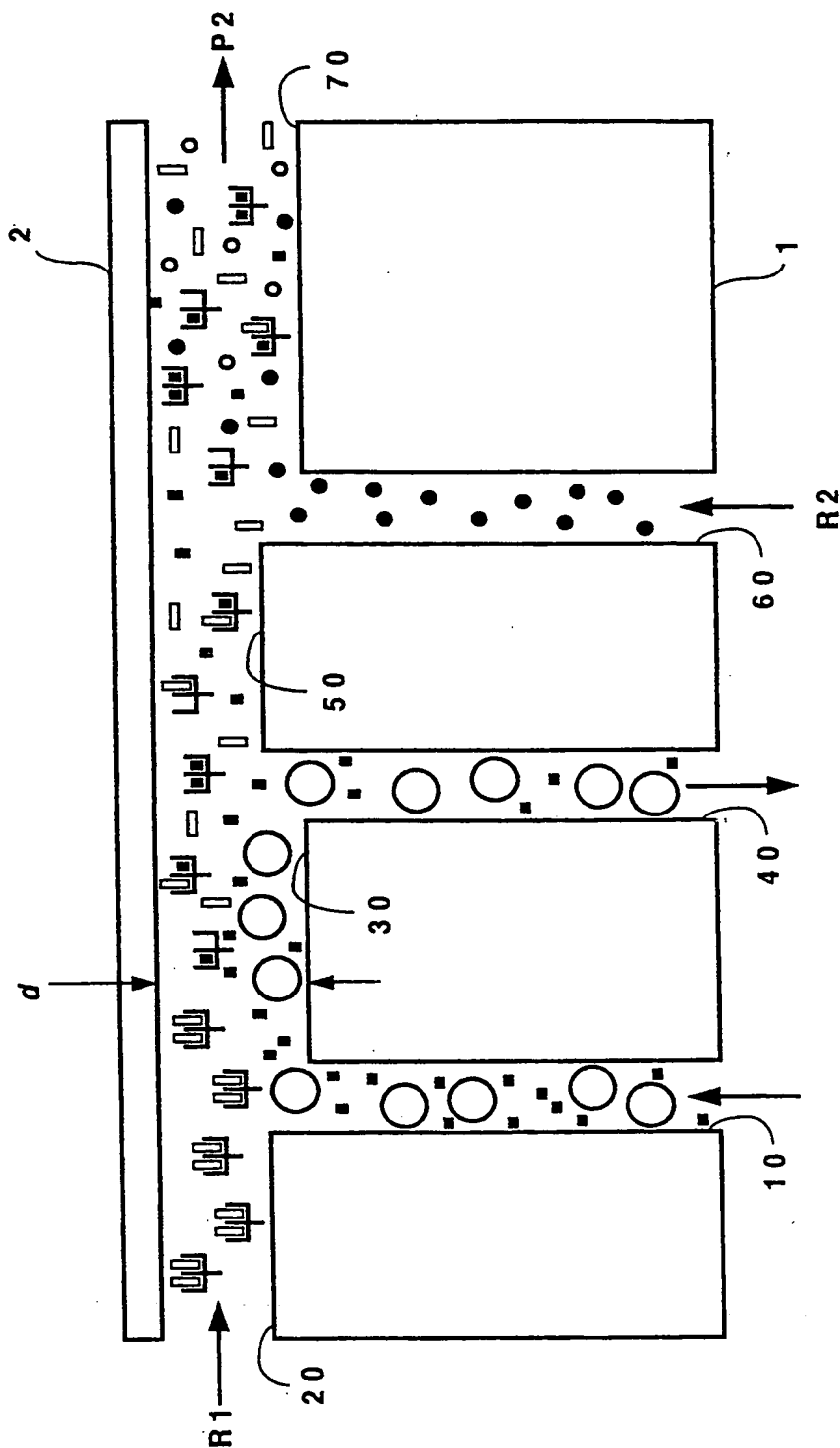


FIG. 13

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US98/19225

A. CLASSIFICATION OF SUBJECT MATTER

IPC(6) : G01N 33/543

US CL : 436/518

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 436/518, 172; 435/6

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

APS, DIALOG

search terms: laminar flow, microfluid?, particle? or ?sphere? or ?bead?, microchannel?, interact?

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X,P	US 5,716,852 A (YAGER et al) 10 February 1998, see abstract, claims and entire document.	1-34
Y	US 4,962,037 A (JETT et al) 09 October 1990, see abstract, column 4, lines 6-16, column 7, lines 40-64, and entire document.	1-5, 9-15
X	US 5,427,946 A (KRICKA et al) 27 June 1995, see abstract, figures, claims and entire document.	1, 19
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Y		2-18, 20-34
A	US 5,444,527 A (KOSAKA) 22 August 1995, see abstract, claims and entire document.	1-34
Y	US 5,278,048 A (PARCE et al) 11 January 1994, see abstract, claims, example 17 and 18, see entire document.	1-34

☒ Further documents are listed in the continuation of Box C. ☐ See patent family annex.

* Special categories of cited documents:	*T* later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
A document defining the general state of the art which is not considered to be of particular relevance	*X* document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
E earlier document published on or after the international filing date	*Y* document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
L document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)	*A* document member of the same patent family
O document referring to an oral disclosure, use, exhibition or other means	
P document published prior to the international filing date but later than the priority date claimed	

Date of the actual completion of the international search

30 DECEMBER 1998

Date of mailing of the international search report

22 FEB 1999

Name and mailing address of the ISA/US
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INTERNATIONAL SEARCH REPORT

 International application No.
 PCT/US98/19225

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X -- Y	US 5,156,039 A (GIDDINGS) 20 October 1992, see abstract, claims, figures and entire document.	19 ----- 1-7, 14-15, 20-24
Y	US 5,039,426 A (GIDDINGS) 13 August 1991, see abstract, figures, claims and entire document.	21-28, 31-34
Y	US 4,737,268 A (GIDDINGS) 12 April 1988, see abstract, figures, claims and entire document.	1-34
X	LEVIN, S. et al. Analytical SPLIT fractionation in the diffusion Mode Operating as a Dialysis-like system of membrane. Application to Drug-Carrying Liposomes. Analytical Chemistry, 17 September 1993, Vol. 65, No. 17, pages 2254, 2261, especially page 2255, Figure 1.	19
Y	WO 93/22053 A1 (TRUSTEES OF THE UNIVERSITY OF PENNSYLVANIA) 11 November 1993, see abstract, claims and entire document.	1-34
Y,P	US 5,750,063 A (HOYT) 12 May 1998, see abstract, claims and entire document.	1-34
Y,P	US 5,726,404 A (BRODY) 10 March 1998, see abstract, claims and entire document.	1-34
Y,P	US 5,726,751 A (ALTENDORF et al) 10 March 1998, see abstract, claims and entire document.	1-34
X	US 4,894,146 A (GIDDINGS) 16 January 1990, see abstract, figures, claims and entire document.	19
Y,P	US 5,674,743 A (ULMER) 07 October 1997, see abstract, figures, claims and entire document.	1-34
Y	WO 96/04547 A1 (LOCKHEED MARTIN ENERGY SYSTEMS INC.) 15 February 1996, see abstract, claims and entire document.	1-34
X	WO 95/27210 A1 (DANFOSS) 12 October 1995, see abstract, claims and entire document.	1-11, 15, 19-24
X,P ---- Y,P	US 5,747,349 A (van DEN ENGH et al) 05 May 1998, see abstract, claims and entire document.	1-6, 9-12, 14-17 ----- 19-27, 30-34, 18

INTERNATIONAL SEARCH REPORT

International application No.
PCT/US98/19225

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y,P	US 5,726,751 A (ALTENDORF et al) 10 March 1998, see abstract, claims and entire document.	19-25
A	US 4,675,300 A (ZARE et al) 23 June 1987, see abstract, claims and entire document.	1-34